

Simulations of ion beams using Geant4 and Fluka Monte Carlo codes

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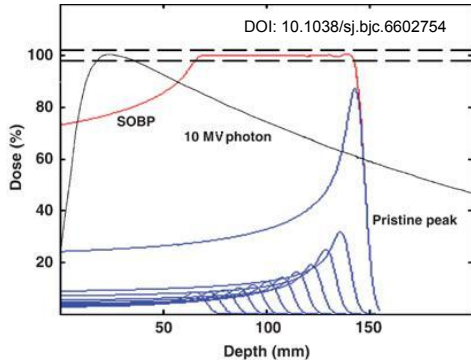
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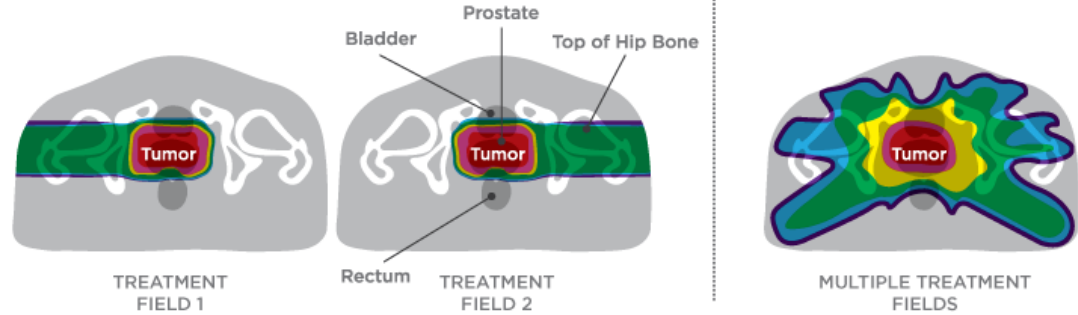


Cancer treatment by hadron therapy

PROTONS



Depth-dose distribution of ions with initial energies 20-300 MeV results in **Bragg peak** curve

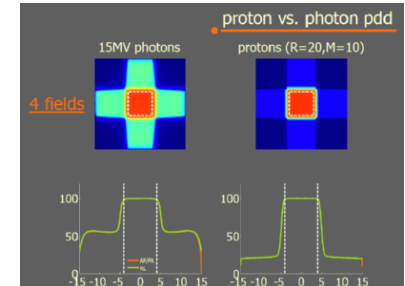


These images show the areas exposed to radiation during treatment.

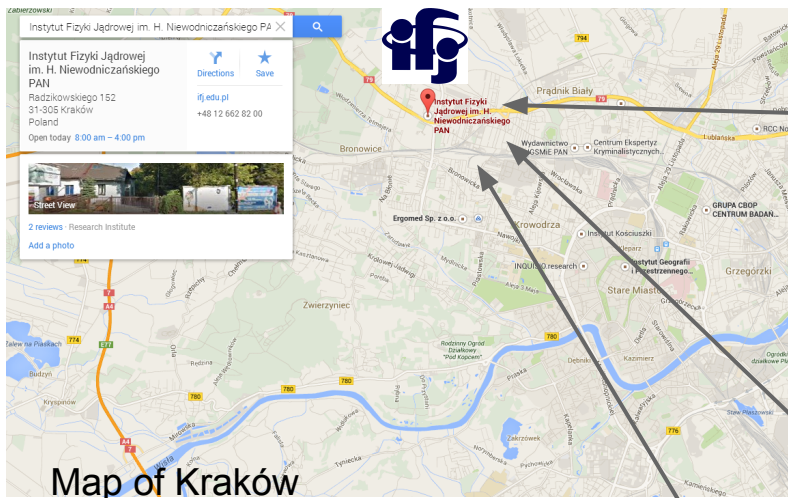
LESS RADIATION MORE RADIATION

http://provisionha.com/images/uploads/multi_site/ProstateCancer_graphic.png

Golden rule of radiotherapy:
to **minimize** the radiation dose to normal tissues while **maximizing** the radiation dose to the target volume.



Cyclotron Centre Bronowice



cyclotron AIC-144
60 MeV protons
80 nA intensity
2.9 cm range in water (max)

eye tumours treatment
isotope production

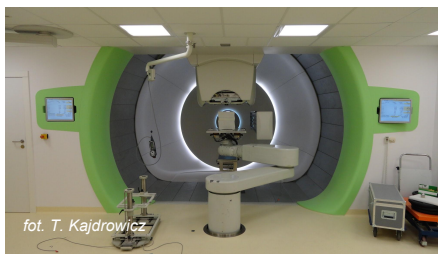
http://www.dziennikpolski24.pl/artykul/2944382_protonami-w-nowotwory.id.t.html



cyclotron Proteus C-235
230 MeV protons
600 nA intensity
33 cm range in water

eye tumours treatment
gantry (x2): any tumor location
experimental cave

http://www.ifj.edu.pl/ccb/img/cyklotron_Proteus235



**two robotic
gantry arms,
scanning
beam**

fot. T. Kajdrowicz



fot. M. Ptaszkiewicz

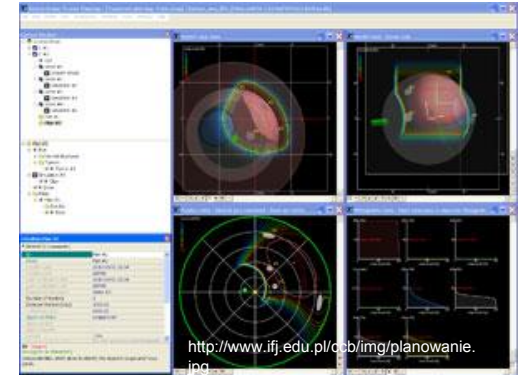
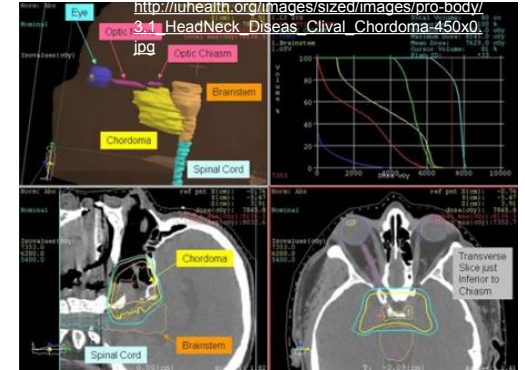
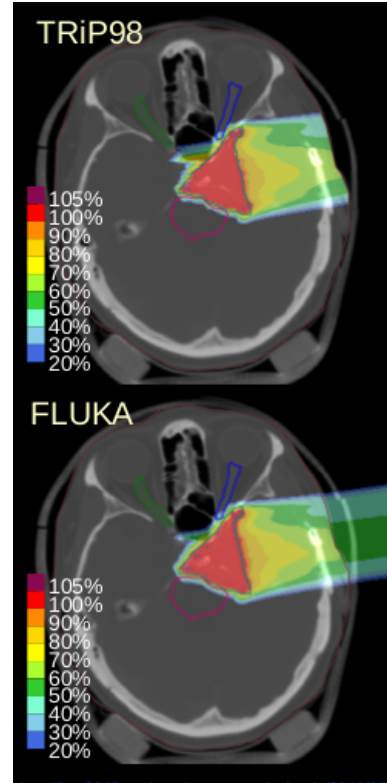
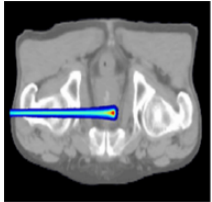
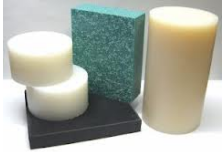
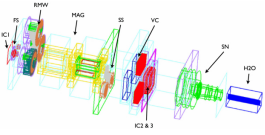
Why do we need a physical beam model ?

optimization of beam scattering system

patient shielding design and verification

verification of treatment plans

simulation of experiments (TLD, alanine)



<http://iccr2013.org/cms/wp-content/uploads/2013/05/Urzsula-Jelen.pdf>

<http://www.ifj.edu.pl/cbb/img/planowanie.jpg>

Monte Carlo Simulation of a proton beam

Aim:

- simulate proton beam:
- dose and fluence profiles (depth, lateral)
 - complex geometry

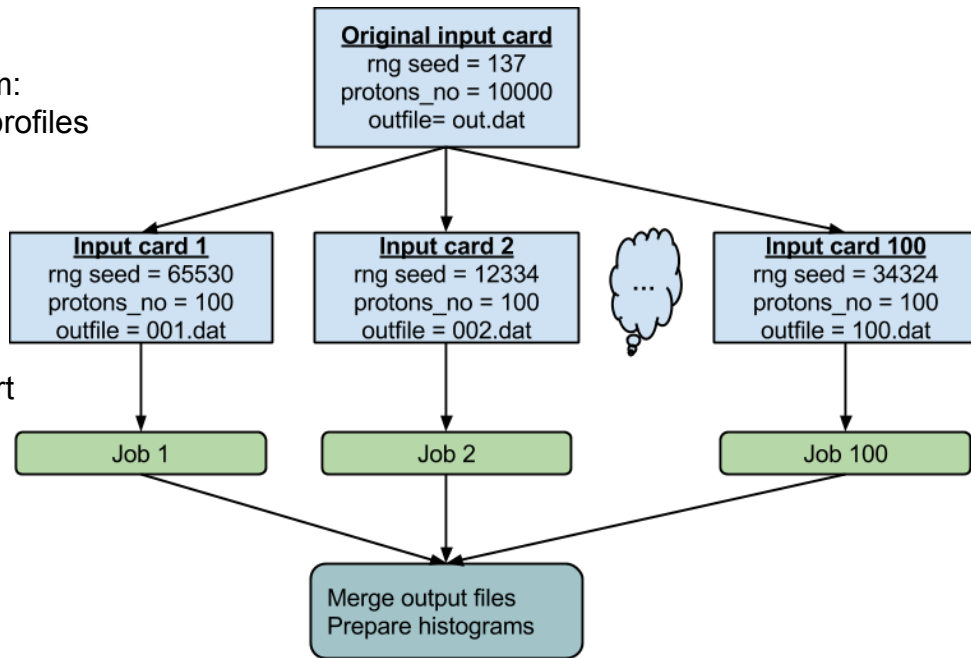
Tools:

Monte Carlo transport codes:

- Fluka 2011.2
- Geant4.96

Results:

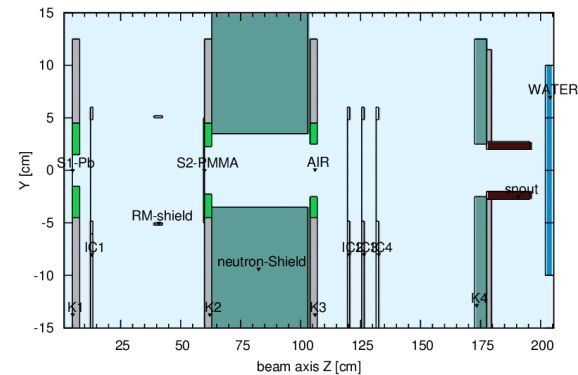
(following page))



Parallelization procedure



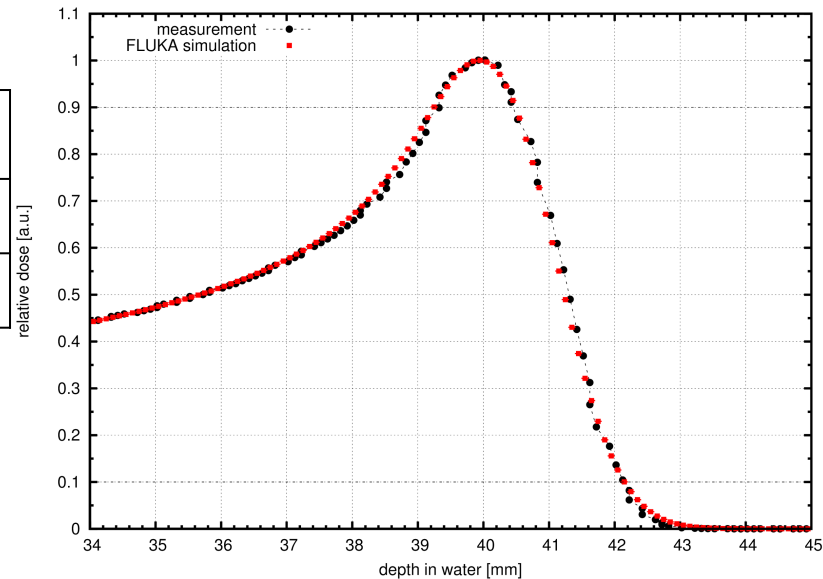
Eye-line scattering system in the treatment room (top) and defined in simulation geometry (bottom)



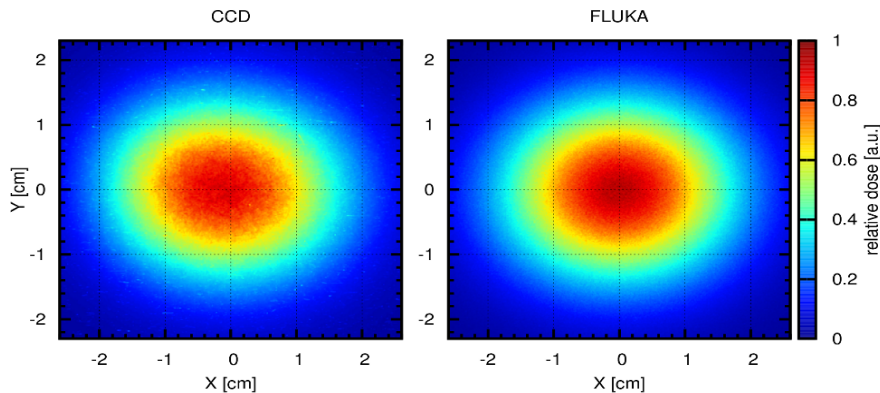
Monte Carlo simulation of a 70 MeV proton beam

Parallelization of an exemplary simulation scenario:

| No of protons x No of jobs | Mean calc. time | Result error |
|----------------------------|-----------------|--------------|
| $2.0 \cdot 10^5 \times 5$ | 10 min/job | 15% |
| $5.5 \cdot 10^6 \times 25$ | 120 min/job | 1% |



Measured depth-dose distribution (black) compared with FLUKA results (red)



CCD beam image (left) compared with FLUKA results (right)

Monte Carlo simulation of a carbon beam

Aim:

scoring beam characteristic in liquid water

- dose (vs depth)
- fluence (vs depth)
- energy-fluence spectra of all ions (vs depth)

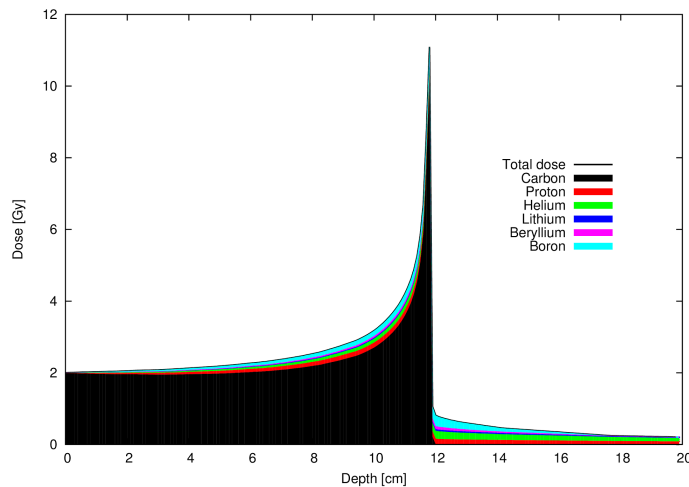
Tools:

Monte Carlo transport codes

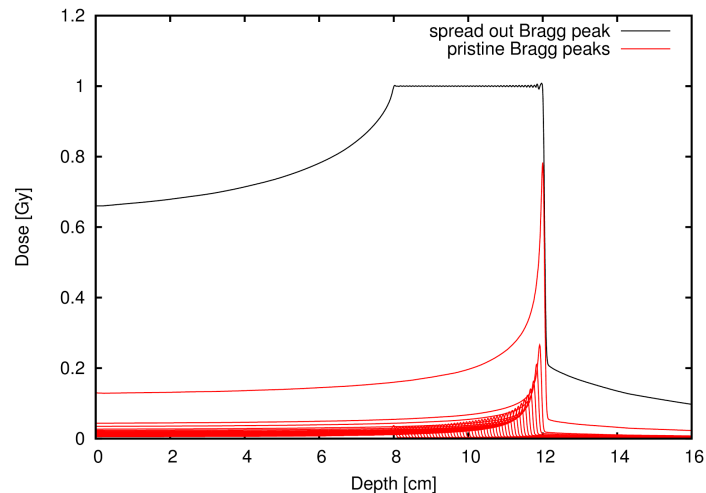
- SHIELD-HIT10
- Geant4.96

Results:

database of 45 beam profiles for initial energies between 50 and 400 MeV/amu



Dose vs depth of a carbon beam of 270 MeV/amu initial energy and of beam fragments.



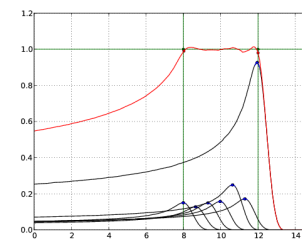
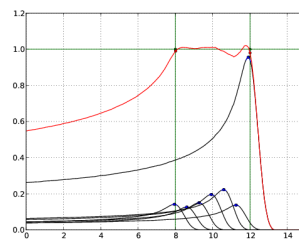
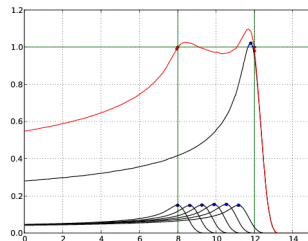
Flat depth-dose distribution over 8-12cm depth range obtained by summation of 49 pristine carbon beams with different initial energies and fluences.

| No of particles | Total calc. time | Number of nodes |
|-----------------|------------------|-----------------|
| 10^4 | 10 min | 1 |
| 10^8 | 70 days | 1 |
| 10^8 | 17 hours | 100 |

Optimization of the depth dose distribution:

Aim:

find the initial energies and intensities of the beamlets which, superimposed, produce a given depth-dose (depth-survival) profile



First three steps of the dose profile optimization algorithm.

Tools:

optimization package included in the libamtrack library (python,C)

Results:

several projects of beam shaping elements
depth-dose and depth-survival profiles
(radiobiological experiment)

Pristine beams superposition:

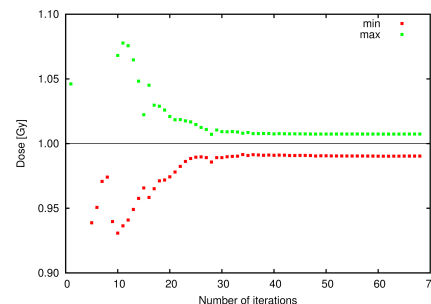
$$f(x; p_1, \dots, p_m, h_1, \dots, h_m) = \sum_{i=1}^m h_i f(x; p_i)$$

Objective function:

$$M = \sum_{j=1}^n \left(f(x_j; p_1, \dots, p_m, h_1, \dots, h_m) - g(x_j) \right)^2$$

Gradient of objective function:

$$\frac{\partial M}{\partial h_i} = \sum_{j=1}^n 2 \left(\sum_{i=1}^m h_i f(x_j; p_i) - g(x_j) \right) f(x_j; p_i)$$

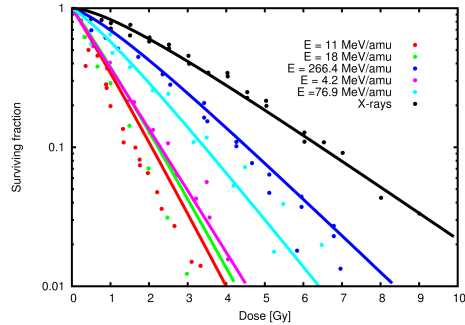


Convergence of the dose profile optimization algorithm.

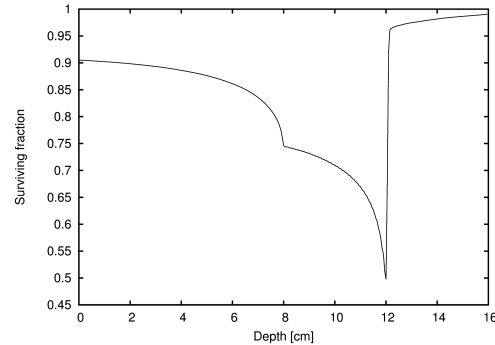


Modelling of biological effect: carbon beams

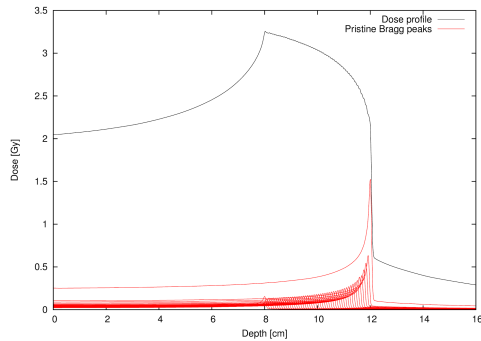
1. Cell survival at given dose depends on the particles energy



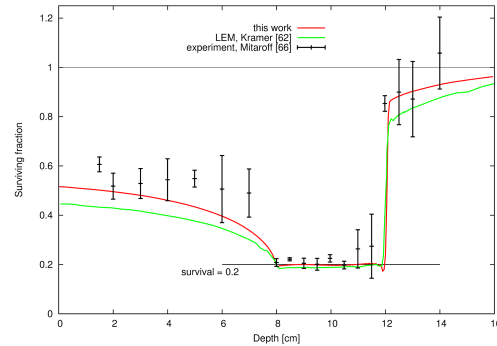
2. Constant dose level of carbon ions leads to non-uniform cell survival



3. Specific depth-dose distribution is needed to obtain constant biological effect of carbon ions



4. Predicted cell survival profile stays in agreement with experimental results



Questions, comments ?



http://naukawpolsce.pap.pl/fotogalerie/gallery_57.montaz-cyklotron-proteus-c-235.html

<http://www.ifj.edu.pl/ccb/>

<https://libamtrack.dkfz.de/>

Thank you and we ask for more !!!

